

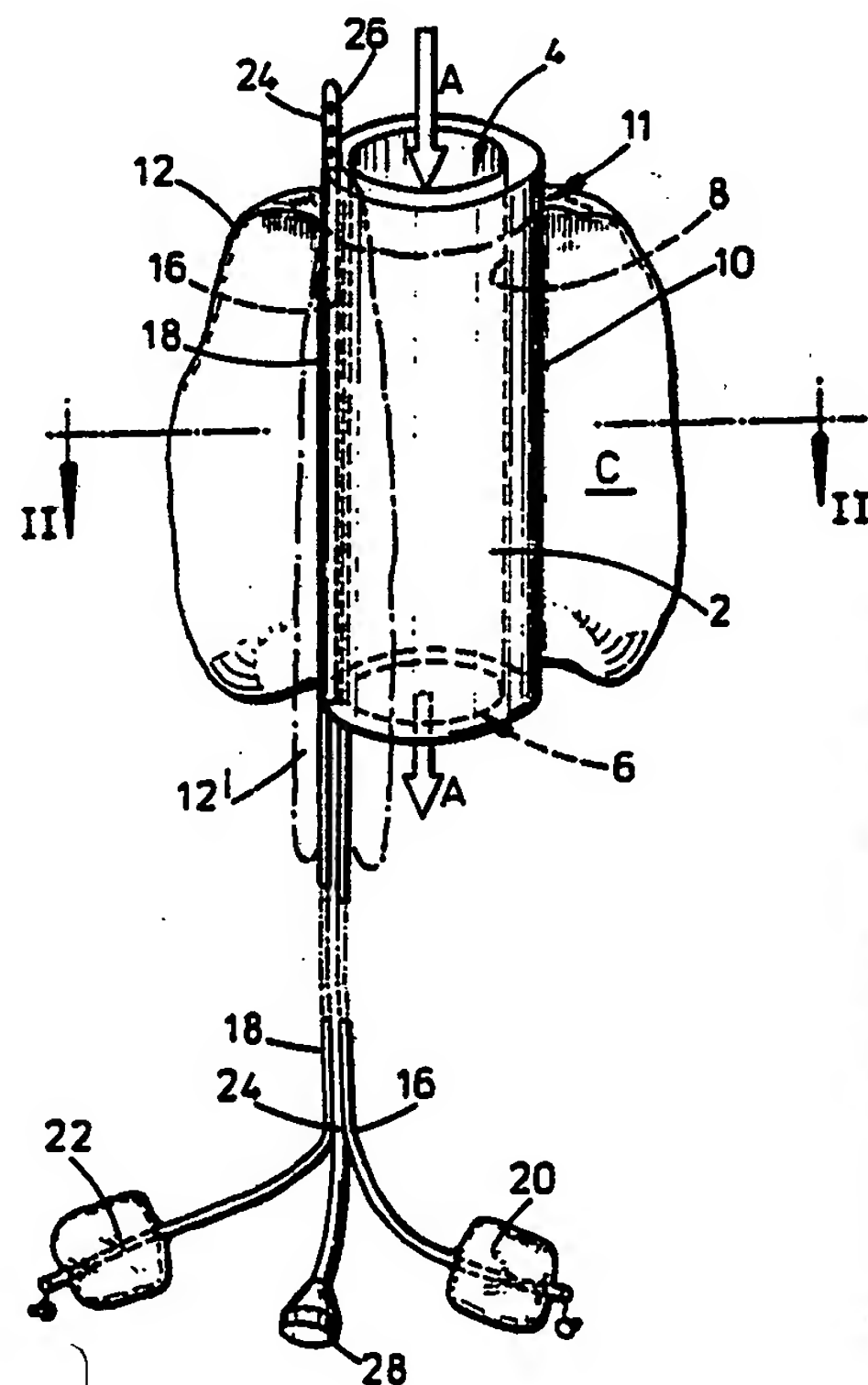


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(21) International Application Number: PCT/GB90/01871 (22) International Filing Date: 30 November 1990 (30.11.90) (30) Priority data: 8927282.7 1 December 1989 (01.12.89) GB (71) Applicant (for all designated States except US): UNIVERSITY OF STRATHCLYDE [GB/GB]; McCance Building, 16 Richmond Street, Glasgow G1 1XQ (GB). (72) Inventor; and (75) Inventor/Applicant (for US only) : LAZIM, Taha, Roudan [GB/GB]; Roudan Cottage, Cadwell Estate, Gleniffer Road, Uplawmoor, Glasgow G78 4BS (GB).		(74) Agents: McCALLUM, William, Potter et al.; Cruikshan & Fairweather, 19 Royal Exchange Square, Glasgow G3AE (GB). (81) Designated States: AT (European patent), BE (European patent), CH (European patent), DE (European patent), DK (European patent), ES (European patent), FR (European patent), GB (European patent), GR (European patent), IT (European patent), JP, LU (European patent), NL (European patent), SE (European patent), US. Published <i>With international search report.</i> <i>Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i>

(54) Title: VASCULAR SURGICAL DEVICES**(57) Abstract**

The invention relates to a surgical device for use in operative substitution or replacement for a damaged or malformed body conduit or blood vessel, an example being an aortic aneurysm. One example described in the specification comprises a tubular body (2) having open-end portions (4, 6) to provide a passageway (A). The wall of the body (2) when inflated comprises an annular chamber (B). Surrounding the body (2) is an outer chamber (C) comprising a flexible sleeve member (12). A probe (24) is provided which extends forwardly of the leading end (4) of the body (2), the probe providing sampling apertures (26) to allow monitoring of body fluid flow when the device is in place. Further tubes (16 and 18) permit inflation of the chambers (B and C respectively). The above device may be suitable for insertion through the femoral artery, while another example described may be found suitable for insertion into the sub-clavian artery.



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VASCULAR SURGICAL DEVICES

The invention is concerned with improvements in or relating to devices suitable for use in vascular surgery, particularly but not exclusively for use in substitution for or replacement of a damaged or malformed region of vessel or other conduit normally adapted to carry a fluid flow in mammals.

As an example of such damaged or deformed vessels, it has apparently become increasingly common over recent years for patients to suffer dilatation or sacculation of arteries, especially the aorta, to produce aneurysms which are liable to rupture. Unless suitably prompt surgery is performed, the condition is fatal. Another condition which requires surgical attention is the correction of blood flow irregularities caused by fistulae resulting from congenital deformity or from damage occurring to organs and blood vessels. In each of these two examples one of the immediate requirements is to restore a through-flow of fluid through the vessel so that fluid-pressure is not lost through leakage or other unwanted passage from the vessel.

It has generally been considered advantageous to prepare for surgery to repair or replace a region of a damaged vessel by blocking the flow of fluid to the vessel at a point slightly upstream of the region. While it is feasible in some circumstances as part of the surgical procedure to arrange an external by-pass conduit for the

fluid flow during the repair procedure, in others this is virtually impossible to achieve.

While aneurysms may occur at any region of the aorta, those situated below the diaphragm, i.e. the abdominal aortic aneurysms, give the most pressing instances in which urgent surgery should be carried out if the patient is to survive. Nevertheless the general condition of the patient will probably be at a poor level due to deep shock associated with blood loss, anuria and/or low blood pressure.

It is one of the objects of the invention to provide an internal by-pass arrangement capable of maintaining, in the short, medium or long term, a fluid flow normally carried by a region of vessel or conduit rendered more or less incapable of carrying such flow.

It is another object of the invention to provide an insertion device adapted for use to connect two portions of a sound fluid flow passageway which flank a damaged or otherwise unsound region of said passageway.

The invention provides in one of its several aspects a surgical device suitable for insertion into a body fluid passageway to span a damaged or deformed portion thereof by forming communication between two relatively sound portions of said passageway spaced apart by the intervening damaged or deformed region of the passageway, said device comprising a substantially tubular body portion having open end portions, the body portion

comprising a tubular wall arrangement adapted to be in an inoperative, flaccid, condition immediately before use, means being provided for rendering the flaccid wall arrangement into a relatively rigid condition when the device is in position for use within the body fluid passageway.

The invention provides, in another of its several aspects, a surgical device suitable for insertion into a body fluid passageway to span a damaged or deformed portion thereof by forming communication between two relatively sound portions of said passageway spaced apart by the intervening damaged or deformed region of the passageway, said device comprising a substantially tubular body portion having open end portions, and an outer sleeve member secured at one end thereof to the body portion adjacent to one of said open end portions and secured at the other end thereof to the body portion adjacent the second of said open end portions so as to define an annular outer chamber around said body portion, said outer sleeve member being formed from flexible material in order to allow inflation of said annular outer chamber, the body member comprising a tubular wall arrangement adapted to be in an inoperative, flaccid, condition immediately before use, means being provided for rendering the flaccid wall arrangement into a relatively rigid condition when the device is in position for use within the body fluid passageway, means also being provided for the concomitant

inflation of the annular outer chamber.

Advantageously, the tubular wall arrangement of the body member comprises an inner flexible wall portion and an outer, substantially coaxial, wall portion, said wall portions being sealed to each other at end portions thereof to form an annular wall chamber, the means to render the flaccid wall arrangement into a relatively rigid condition comprising inflation means to inflate the annular wall chamber.

Conveniently the outer wall portion of the annular wall chamber is common with and shared by the annular outer chamber, forming its inner surface.

Preferably the annular wall chamber is inflated to a pressure higher than that of the annular outer chamber, the pressure in said outer chamber being such that the sleeve member is readily conformable to the contours of the interior surface of the intervening passageway region.

Desirably, means are also provided whereby the fluid flow through the vessel and the passageway formed by the inflated tubular body portion may be monitored, together with velocity and pressure measurement and the facility of sampling the fluid for subsequent bio-chemical and bio-physical analyses. Conveniently, the monitoring means may include a perforated probe projecting into, for example, the blood passing through an artery or vein. Such a probe may conveniently enter the device through a sealed aperture through which also pass inflation tubes

leading to the inflatable chamber(s).

In an example of a device according to the invention which is to be described below, the tubular wall arrangement comprises an inflatable annular chamber, which is to be inflated to an extent at which it becomes, reasonably rigid, may be prevented from undue distortion or "ballooning" by the provision of ties spanning the annular chamber in a radial manner to link outer and inner wall portions.

Alternatively, the annular chamber comprises a plurality of interconnected longitudinally arranged inflatable channels, conveniently having intervening plain areas.

Devices according to the invention are suitable for use in a wide range of situations. For example, a device may be used to form a conduit or a closure for a fistula which may be of a naturally occurring type such as a vascular defect affecting babies where a pre-birth pulmonary by-pass passage fails to close or, alternatively, requires to be kept open for a certain time. Other examples may be required for use as a result of injury such as a penetrative wound or pathological condition which forms a communication between the trachea and oesophagus or between an artery and a vein.

Alternatively, a device according to the invention may be used to maintain in an open condition a passageway which is at risk from closure due to a pathological

condition.

While it is often convenient for a device according to the invention to be introduced through the femoral artery, it may be preferred to arrange to introduce the device through the sub-clavian artery.

Many of these examples are intended for use as short-term expedients but it is also possible to select material and situations where the device may be retained in place on a more-or-less permanent basis such as in certain forms of vascular aneurysm in the brain and inoperable vascular aneurysms.

However, the example to be described below is in the context of arterial damage, particularly in treating, often on an emergency basis, an aneurysm formed by weakness in the wall of the aorta. Aortic aneurysms may occur at any region of the aorta, those above the diaphragm being referred to as thoracic aortic aneurysms and those below being known as abdominal aortic aneurysms, (A.A.A.).

Aortic aneurysms are frequently the result of the effects of arterio-sclerosis and expanded to the point of rupturing by high blood pressure levels. Thus the condition of the arteries in patients is frequently poor and many patients who receive successful operative treatment for the ruptured aneurysm nevertheless die from myocardial infarction, renal or multiple organ failure especially as emergency surgery is usually carried out on

a patient who is in a state of deep shock.

Correcting the effect of shock due to rupture of the aneurysm is difficult in emergency operations when there is a continuous leakage of blood from the tear in the artery wall at the site of the aneurysm. Many attempts have been made to stem the flow through the aorta long enough to permit the tear to be closed. Devices such as inflatable plugs or catheters inserted into the upstream neck of the aneurysm may be more effective than simply clamping and closing the aorta, but either of these techniques stops the supply of blood to the pelvis and lower limbs. In some cases it is possible during surgery to provide an external by-pass conduit but such procedures do not allow stabilisation of the patient's condition prior to surgery. Serious risks still remain in that shock, metabolic abnormalities or deficiencies in heart, lung and kidney functions are not ameliorated prior to surgery. Similarly, the presently available range of devices does not allow immediate restoration of blood flow to the lower limbs and therefore damage may be still present there after successful surgery.

It would therefore be advantageous for the surgery necessary for repair of the ruptured aneurysm to be delayed until the patient's condition has stabilised and he/she has come out of shock. A device according to the invention may be used to achieve this aim.

There will now be described in detail two examples of

a device according to the invention. It will be understood that the description, which is intended to be read with reference to the drawings, is given by way of example only and not by way of limitation.

In the drawings:-

Figure 1 shows a perspective view partly in section, of the first device in a inflated condition,

Figure 2 is a cross-sectional view on line II - II of Figure 1, to a slightly smaller scale;

Figure 3 is a view similar to that of Figure 2 of a modification of the device;

Figure 4 is a perspective view, partially in section of the device in position in an association with an aortic aneurysm;

Figure 5 shows an alternative constriction of an inner wall portion of the first device;

Figures 6 and 7 are cross-sectional views of the wall portion as shown in Figure 5 and in an alternative construction, respectively;

Figure 8 shows a second example of a device according to the invention; and

Figure 9 is a fragmentary portion of the device of Figure 8 to an enlarged scale.

The first device comprises an inflatable tubular body 2 having open end portions 4, 6 to provide a passageway therethrough in the direction shown by arrows A. The tubular body 2 comprises an inner wall portion 8 and an

outer wall portion 10 which in the present example are of reinforced polyvinylchloride sheet material, each portion being sealed at said end portions to the other portion to form an annular wall chamber B. It will be understood that other bio-compatible materials may also be utilised.

Attached to the outer wall portion 10 at two circumferential regions thereof, each spaced inwardly of the end portions 4, 6 respectively to form a shoulder at 11, is a sleeve member 12 which in the present example is of polyurethane sheet material, and which together with an outer surface wall portion 10 defines an annular outer chamber, C, as shown in Figures 2 and 3.

The chambers are adapted to be inflated as will be explained below, the modification shown in Figure 3 including wall tie members 14 adapted to reduce any tendency for distortion of the chamber B by undue ballooning of the wall portions 8 and 10.

The device described in the present example is provided with two independent inflation means comprising a supply pipe 16 adapted for use in the controlled inflation of chamber B and a supply pipe 18 for the controlled inflation of chamber C. Monitoring sacs 20, 22 allow the user to check the state of inflation from the pipes 16, 18, respectively, although the pipes may be connected to other equipment for accurate measurements of inflation pressures.

The two pipes are formed into an assembly with a

hollow flexible probe 24 comprising a tube having a plurality of sampling apertures 26 at a leading end thereof which conveniently projects beyond the end portion 4 of the wall portions 8, 10 of chamber B so as to have access to the fluid flowing in the direction of arrow A, upstream of the device. Sampling apparatus may be attached to the probe 24 at an outer end 28 thereof. Conveniently the probe arrangement may be used for monitoring blood pressure, taking samples, in angiography, or in association with other sensors.

Figure 4 shows the device in use in a situation involving an abdominal aortic aneurysm. The aorta 30 has formed an aneurysm 32 at a region below the renal arteries 34 and above the bifurcation of the aorta at 36. The aneurysm has a tear 38 in the wall thereof and a quantity of thrombus 40 is present within the aneurysm.

The device is in a completely deflated condition in which both chambers B and C are flaccid, taking up the general outline 12 shown in chain dotted lines in Figure 1. An incision is made in one of the femoral arteries 37 and the device introduced so as to enter the aneurysm. The probe 24 acts to support the flaccid chambers during this procedure, the leading end of the probe acting as a pilot portion. It is convenient if the leading end of the probe is equipped with sensor means to detect the change in blood pressure velocity or pattern of flow at the region of the entrances to the renal arteries to confirm

that the device has been inserted into the required position. However, this is not an essential requirement.

As soon as the surgeon is satisfied that the device is correctly positioned, the chambers B and C may then be inflated. Chamber B is inflated and takes up the desired tubular shape as shown in Figure 4, in which its upper end portion 6 is arranged so that the aorta 30 is substantially or completely blocked by its presence, forcing the blood to flow through the passageway bounded by a tubular wall arrangement which is by now firm and effectively rigid. It will be appreciated that this positioning and blocking is aided by the provision of the shoulder 11 formed at the seam between wall portions 10 and 12.

Inflation of chamber C through the line 18 meanwhile causes the sleeve member 12 to conform to the shape of the aneurysm allowing for the presence of thrombus. Thus the tear 38 is sealed by the wall portion 12 and the aneurysm generally supported by the inflated chamber C. However, chamber C is inflated to a pressure level, say, 20-50mm Hg, less than that required for the chamber B which may be 100-150mm Hg.

Figures 5 to 7 show two alternative forms of construction of chamber B to that illustrated in Figures 1 to 4. Chamber B' comprises an inner wall 42, and an outer wall 44 that is common to the outer chamber C. However, a series of longitudinally disposed, interconnected passages

46 are formed by webs 48 spanning the annular chamber, the passages alone being inflated. It will be observed that the passages 46 are no wider than the intervening areas of wall 42,44. In Figure 7, the passages 46 are defined by intervening solid wall portions 50, the passages 46 comprising the chamber B".

Figure 8 shows an alternative arrangement which is suitable for use in many circumstances and is particularly suitable where the device is introduced through the sub-clavian artery. It appears that the device illustrated has the advantage of minimising the further quantity of blood entering the aneurysm. The device shown in Figure 8 comprises a chamber B" of the construction shown in Figures 5 and 7 comprising passages 46 and having intervening solid wall portions 50. Chamber C' is defined by the outer surface of chamber B" and an outer wall 52 which is flexible but substantially inelastic. It is arranged that chamber B" projects at each end, beyond the chamber C. The shape of the wall 52, when inflated gives an area of widest diameter at 54 (approximately 55mm in one example) tapering downwardly to about 30mm at the area 56. It will be observed that the widest diameter at 54 is approximately at a level one third of the distance (60mm) from the leading end 58 of the device to the trailing end 60. It has been found that the formation of the chamber at 54 tends to prevent displacement of the device in use, by normal blood flow.

The inflation and sampling means of Figures 8 and 9 will now be described. This comprises a supply pipe 62 for inflating the passages 46 of chamber B" and a supply pipe 64 for inflating the chamber C. Each pipe 62, 64 is provided with a one-way valve 66,68, at a region adjacent a joining zone between the pipes 62 and 64 and extensions 70 and 72 which are connected at their remote ends to a source of CO₂ gas. A sampling probe 74, the leading end 76 of which projects beyond the leading edge 58 of the device, is also provided with an extension 78, the three extensions being joined by suitable means at 80. It will be understood that the extension 78 is provided at its remote end with a sampling connector to attach to a clinical syringe.

It is important to note the possible advantages which may accrue from the use of flexible but relatively inelastic material for the chamber walls. Thus the shape of the chamber C' when inflated may be carefully controlled as to contour and size by its actual manufacture rather than by the degree of inflation to which it is subjected.

The device thus forms an internal by-pass for the aortic blood flow and may remain in place temporarily at least until the condition of the patient has stabilised so that conventional surgical techniques may be applied, for example the replacement of the damaged region of the vascular wall by a graft of suitable plastics material.

If, however, the patient's condition is such that further surgery is inadvisable, then the device according to the invention may remain in place for a much longer period. Suitable materials will be chosen to permit such an option to be available, that is, materials which do not cause adverse reaction when in situ. Where the device is intended to be effectively permanent, the conduit holding the lines 16 and 18, together with the monitoring probe, may be disconnected at a suitable location.

In the above example a device has been described which includes two inflatable chambers, one inflated to a pressure level such that a reasonably rigid tubular passageway is achieved and the other, surrounding the first, to assist in sealing and supporting damaged areas. It will be understood that in situations in which it is necessary simply to provide a passageway to replace a section of body conduit, only one tubular chamber need be provided.

Various modifications may be made within the scope of the invention as defined by the following claims.

CLAIMS:

1. A surgical device suitable for insertion into a body fluid passageway to span a damaged or deformed portion thereof by forming communication between two relatively sound portions of said passageway spaced apart by the intervening damaged or deformed region of the passageway, said device comprising a substantially tubular body portion having open end portions, the body portion comprising a tubular wall arrangement adapted to be in an inoperative, flaccid, condition immediately before use, means being provided for rendering the flaccid wall arrangement into a relatively rigid condition when the device is in position for use within the body fluid passageway.
2. A surgical device suitable for insertion into a body fluid passageway to span a damaged or deformed portion thereof by forming communication between two relatively sound portions of said passageway spaced apart by the intervening damaged or deformed region of the passageway, said device comprising a substantially tubular body portion having open end portions, and an outer sleeve member secured at one end thereof to the body portion adjacent to one of said open end portions and secured at the other end thereof to the body portion adjacent the second of said open end portions so as to define an annular outer chamber around said body portion, said outer sleeve member being formed from flexible material in order

to allow inflation of said annular outer chamber, the body member comprising a tubular wall arrangement adapted to be in an inoperative, flaccid, condition immediately before use, means being provided for rendering the flaccid wall arrangement into a relatively rigid condition when the device is in position for use within the body fluid passageway, means also being provided for the concomitant inflation of the annular outer chamber.

3. A device as claimed in either one of claims 1 and 2, wherein the tubular wall arrangement of the body member comprises an inner flexible wall portion and an outer, substantially coaxial, wall portion, said wall portions being sealed to each other at end portions thereof to form an annular wall chamber, the means to render the flaccid wall arrangement into a relatively rigid condition comprising inflation means to inflate the annular wall chamber.

4. A device as claimed in claim 3 wherein the inner wall portion and the outer wall portion are connected together at intervals by web portions spanning the wall portions.

5. A device as claimed in claim 4, wherein the web portions are arranged to provide a series of longitudinally disposed, interconnected passages.

6. A device as claimed in claim 2, wherein the tubular wall arrangement of the body member comprises a flexible wall portion having passages formed therein with intervening solid wall portions, the means to render the

body member into a relatively rigid condition comprising inflation means to inflate the passages in the flexible wall portion.

7. A device as claimed in claim 2, and in any one of claims 3 to 6 insofar as they are dependent on claim 2, wherein the outer wall portion of the annular walled chamber is common with and shared by the annular outer chamber, forming its inner surface.

8. A device as claimed in claim 7, wherein the material from which the outer chamber is formed is readily conformable in use to the contours of the interior surface of said intervening body fluid passageway region.

9. A device as claimed in claim 7, wherein the material from which the outer chamber is formed is inelastic.

10. A device as claimed in claim 9, wherein the outer chamber in its inflated condition adopts a double-cone configuration in which the largest diameter thereof is at the annular region when the bases of both cone configurations merge together.

11. A device as claimed in any one of the preceding claims, in which the monitoring means includes a perforated probe projecting beyond leading end portion of the device and including a tubular conduit to a sampling apparatus.

12. A device as claimed in claim 11, wherein the probe provides support for the inflation means.

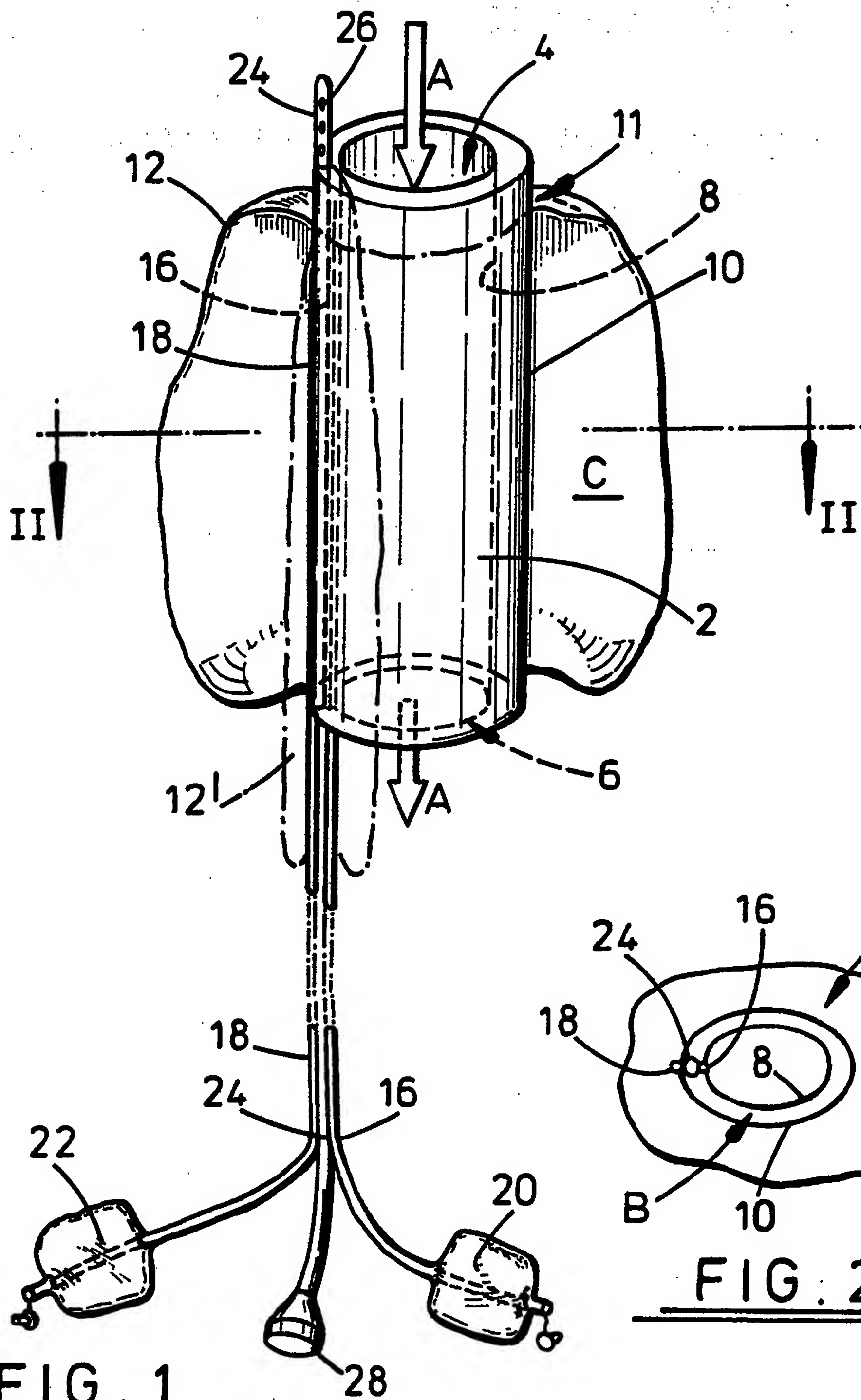
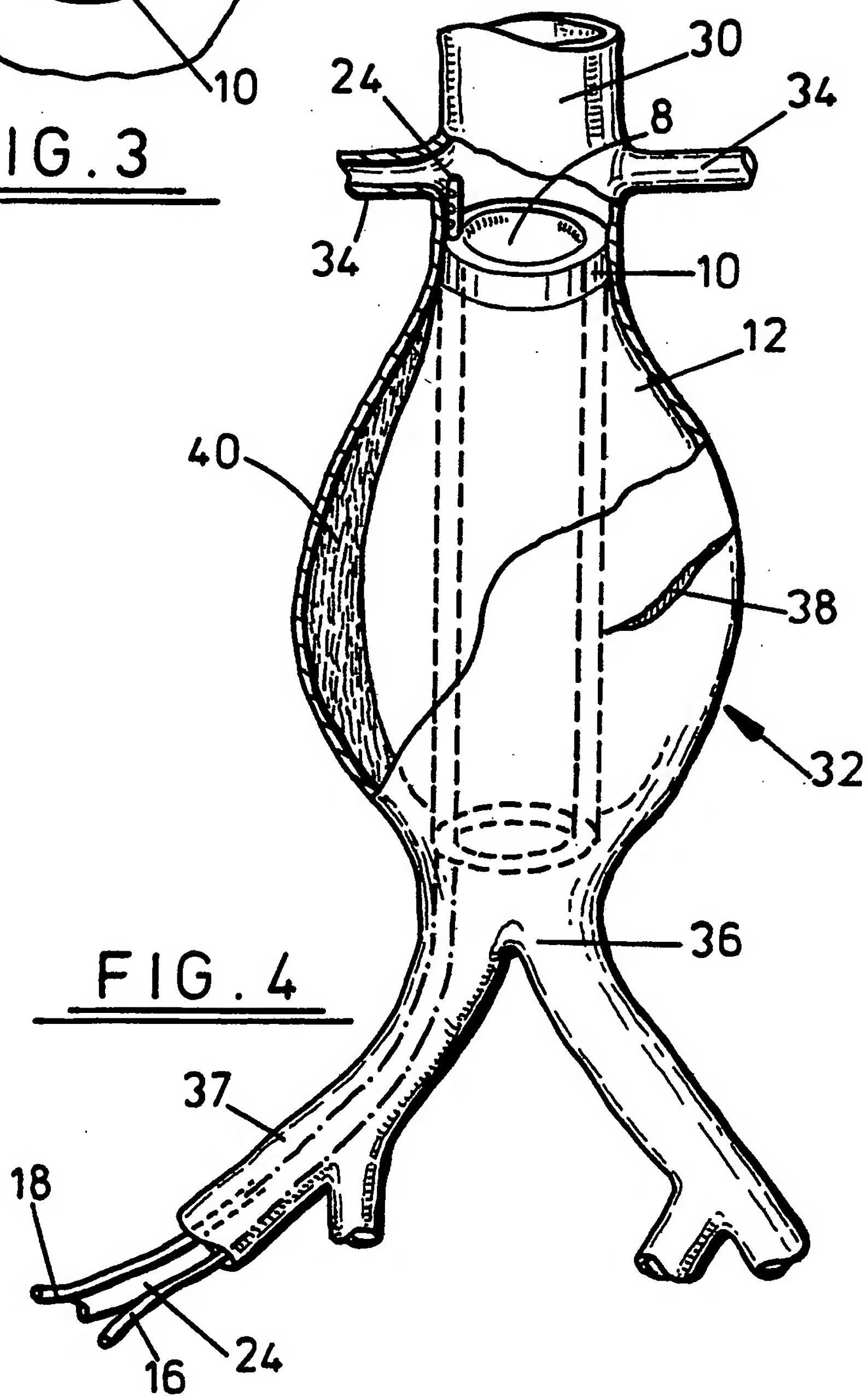
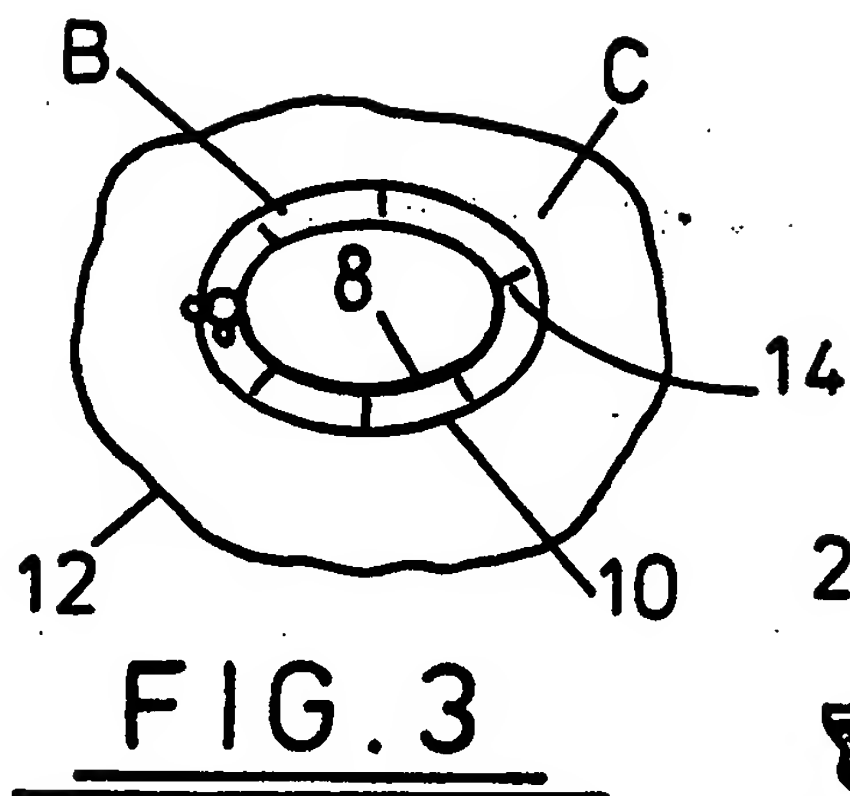


FIG. 1

FIG. 2



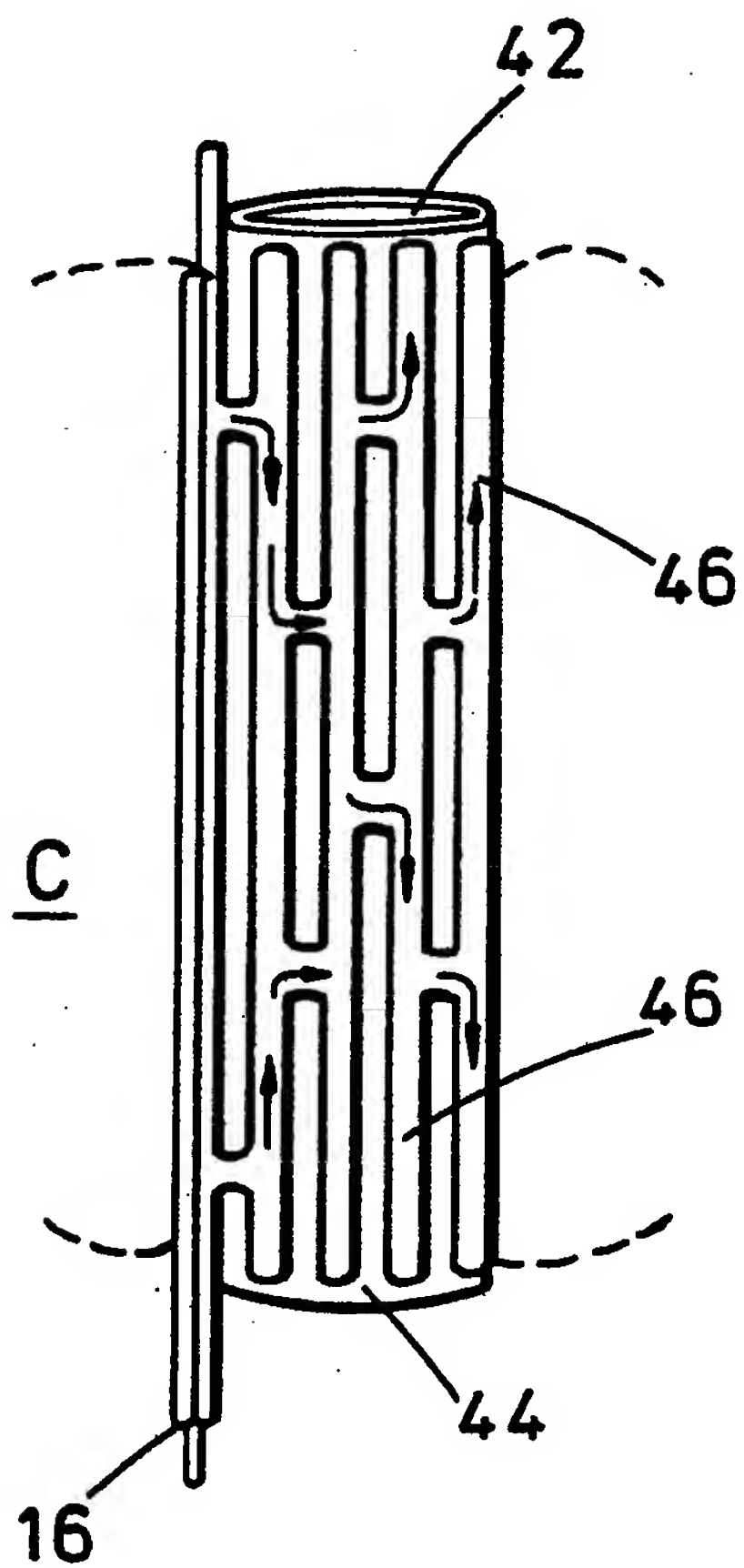


FIG. 5

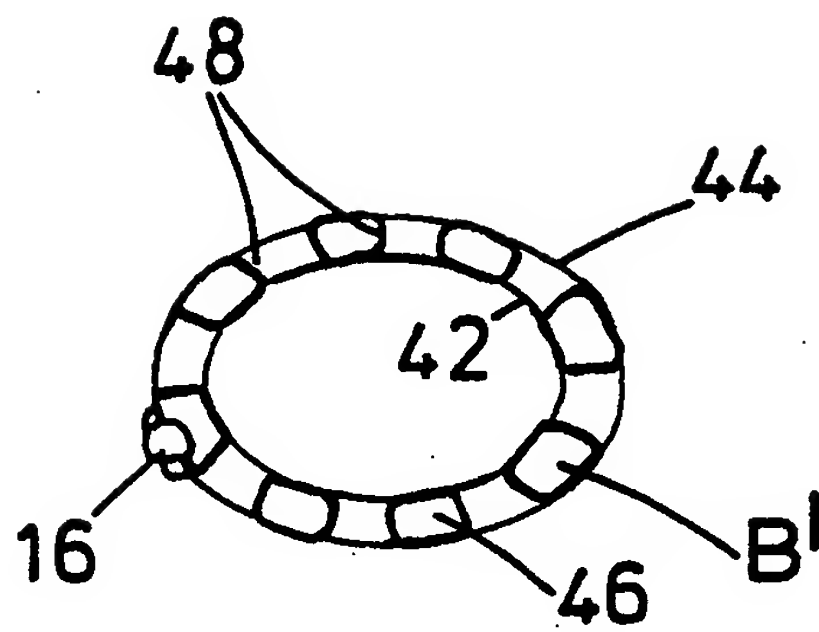


FIG. 6

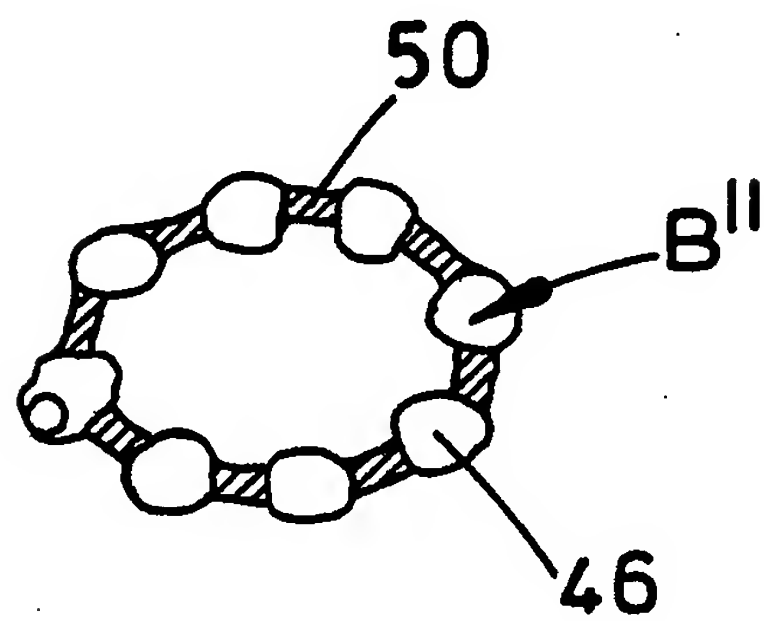


FIG. 7

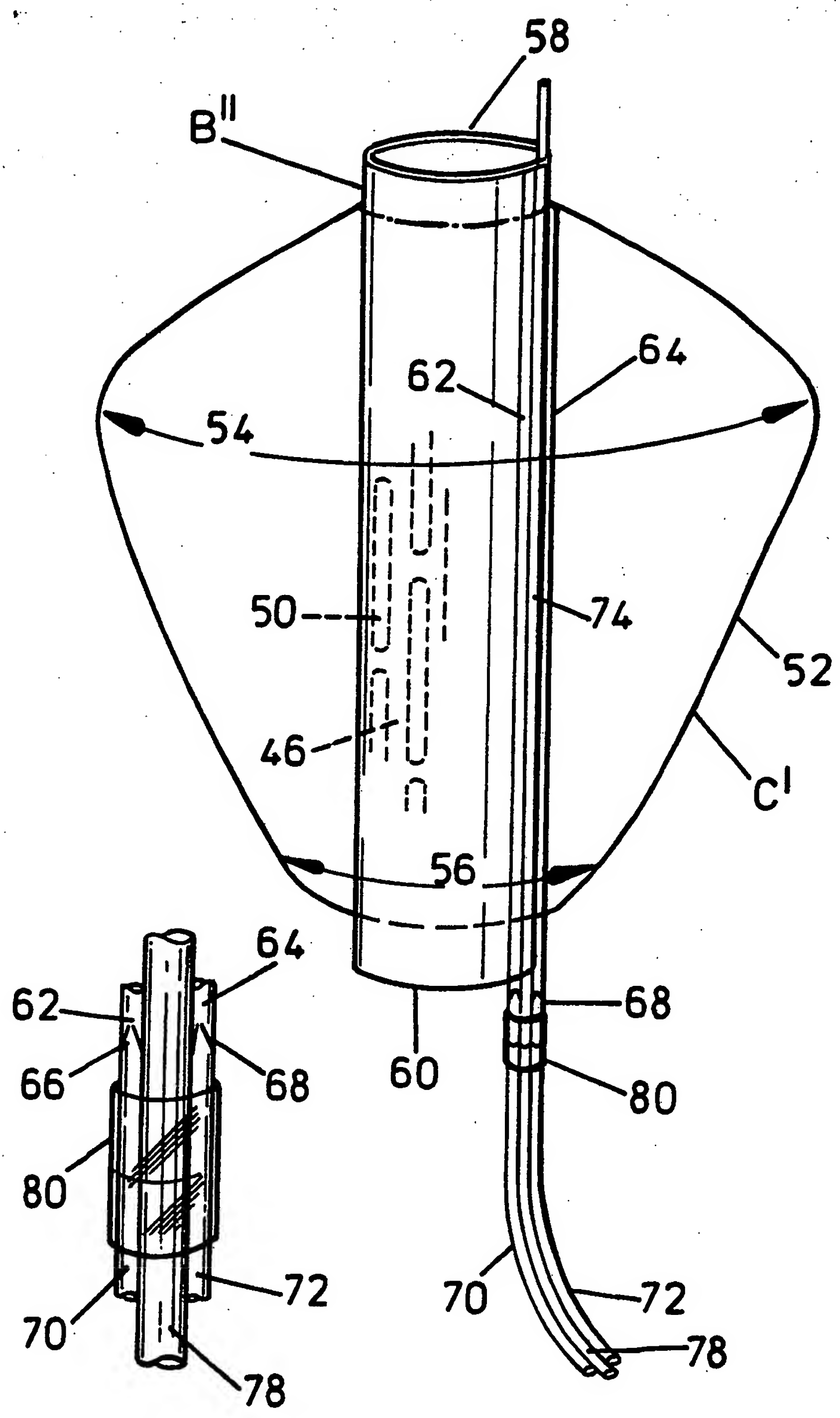
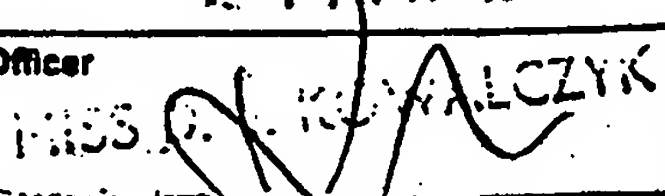


FIG. 9

FIG. 8

INTERNATIONAL SEARCH REPORT

International Application No **PCT/GB 90/01871**

I. CLASSIFICATION OF SUBJECT MATTER (If several classification symbols apply, indicate all) *		
According to International Patent Classification (IPC) or to both National Classification and IPC		
IPC⁵: A 61 F 2/02, A 61 F 2/06		
II. FIELDS SEARCHED		
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Classification System	Classification Symbols	
IPC⁵	A 61 F, A 61 B	
Documentation Searched other than Minimum Documentation to the Extent that such Documents are Included in the Fields Searched *		
III. DOCUMENTS CONSIDERED TO BE RELEVANT *		
Category *	Citation of Document, ¹¹ with Indication, where appropriate, of the relevant passages ¹²	Relevant to Claim No. ¹³
X	US, A, 4183102 (GUISET) 15 January 1980 see column 2, line 31 - column 5, line 50; column 6, line 17 - column 8, line 39; figures 1-6,8,9	1,3-5
A	---	2,6-12
A	US, A, 3435824 (GAMPONIA) 1 April 1969 see column 2, line 27 - column 4, line 16; figures 1,2	2
A	US, A, 4705517 (DIPISA) 10 November 1987 -----	
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IV. CERTIFICATION		
Date of the Actual Completion of the International Search		Date of Mailing of this International Search Report
25th February 1991		14 APR 1991
International Searching Authority		Signature of Authorized Officer
EUROPEAN PATENT OFFICE		

**ANNEX TO THE INTERNATIONAL SEARCH REPORT
ON INTERNATIONAL PATENT APPLICATION NO.**

**GB 9001871
SA 42334**

This annex lists the patent family members relating to the patent documents cited in the above-mentioned international search report.
The members are as contained in the European Patent Office EDP file on 19/03/91
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Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US-A- 4183102	15-01-80	None	
US-A- 3435824	01-04-69	None	
US-A- 4705517	10-11-87	None	

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